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# Stress Corrosion Testing of Mg Wire

Adam Griebel, Alexis Nicolette-Baker,  
Anh Pham, Sam Friedman, Jeremy Schaffer

Updates in Bioabsorbable Metals 2020 | August 25, 2020 | Virtual



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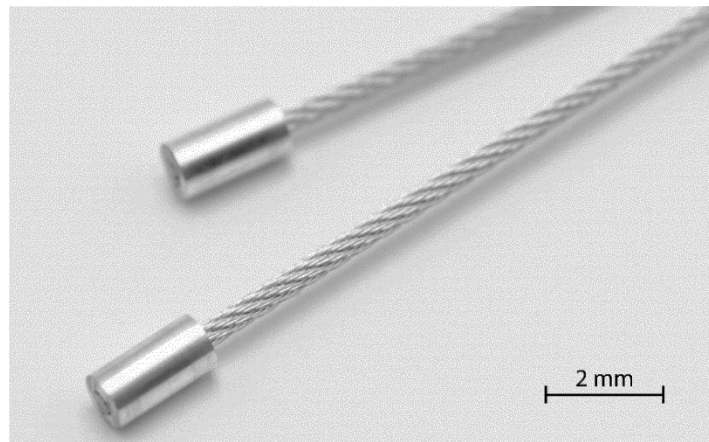


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# Absorbable Wire in Medicine

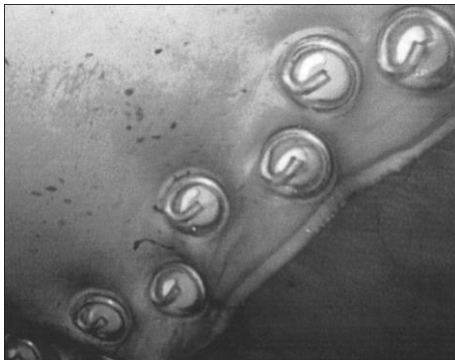
Orthopedic devices (cables, screws, pins, etc.)



# Absorbable Wire in Medicine

Orthopedic devices (cables, screws, pins, etc.)

Soft Fixation (staples, ligation, sutures)

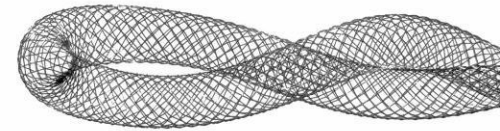
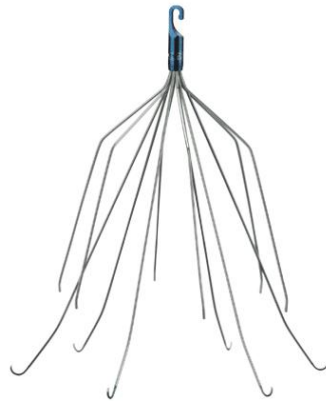
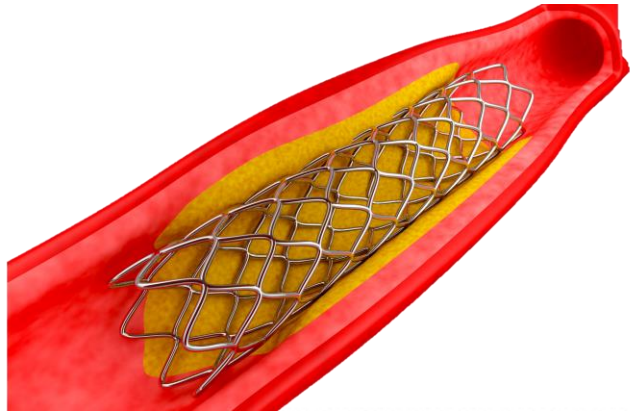


# Absorbable Wire in Medicine

Orthopedic devices (cables, screws, pins, etc.)

Soft Fixation (staples, ligation, sutures)

Stents and intraluminal scaffolds





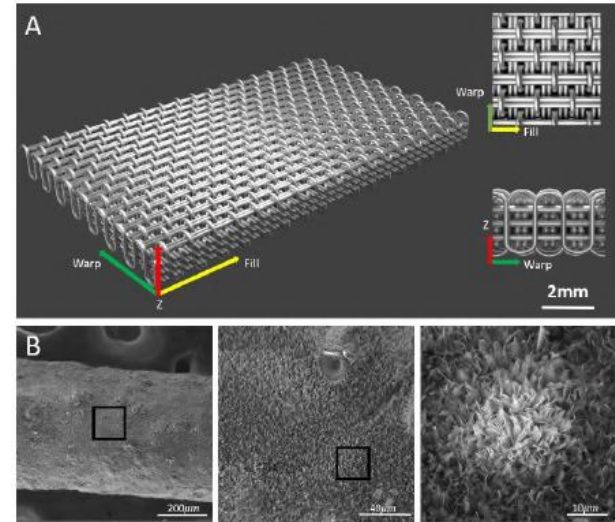
# Absorbable Wire in Medicine

Orthopedic devices (cables, screws, pins, etc.)

Soft Fixation (staples, ligation, sutures)

Stents and intraluminal scaffolds

Scaffolds



*Fig. 1: (A) schematic of Mg 3D weave; (B) Mg alloy wire coated with HAp*

*Xue et al, Biometal 11, (2019)*

# Mg wire in medicine

## 1924

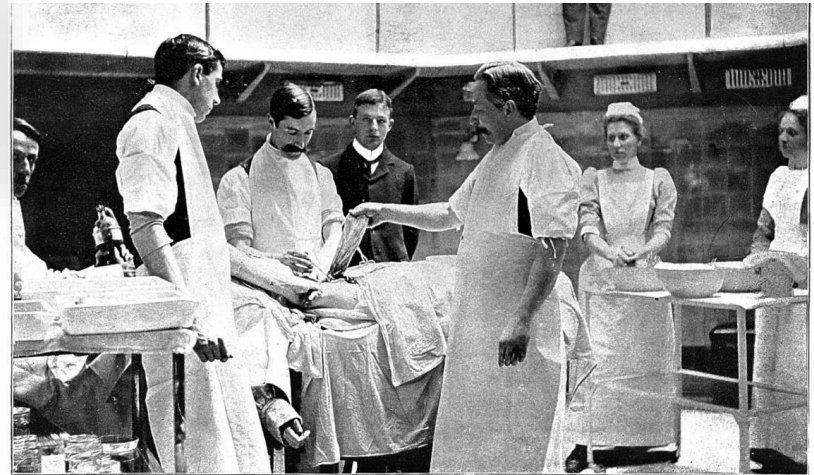
A STUDY OF MAGNESIUM WIRE AS AN ABSORBABLE  
SUTURE AND LIGATURE MATERIAL\*

M. G. SEELIG, M.D.

ST. LOUIS

In adapting the metal for this purpose, there were several requirements to be met:

1. A wire of sufficient tensile strength to withstand the strain of sewing and tying.
2. A wire of sufficient pliability or ductility to withstand the flexing encountered in tying the surgeon's double knot.
3. A wire of high and uniform purity to insure corrosion taking place uniformly when in contact with blood serum.
4. A wire permitting some measure of control in the rate of absorption.



# Why do we do corrosion testing?





# Why do we do corrosion testing?

- Screen
  - Which alloys might work?
  - Which alloys will not work?
- Optimize
  - Which composition/process/surface works best?
- Inspect/Verify
  - How repeatable is it?
  - Did this batch meet our requirements?
- Answer fundamental questions
  - What factors influence corrosion, and how can we control them?
  - What is the corrosion mechanism?
- Predict *in vivo* performance?



# Corrosion Assessment

- Electrochemical (PDP, EIS)
- Immersion
- Stress Corrosion
- Corrosion Fatigue



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## New approaches in evaluating metallic candidates for bioabsorbable stents

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Associate Professor, Department of Biomedical Engineering Michigan Technological University Houghton, MI, USA

European Cells and Materials Vol. 26. Suppl. 5, 2013 (page 28)

ISSN 1473-2262

**Effect of stress on the corrosion behaviour of magnesium wire in m-SBF**S Zhang<sup>1</sup>, X Li<sup>2</sup>, H Wu<sup>2</sup>, C Zhao<sup>2</sup>, J Liu<sup>1</sup>, Y Zhang<sup>1</sup>, X Zhang<sup>1,2</sup><sup>1</sup>Suzhou Origin Medical Technology Co., Ltd. <sup>2</sup>School of Materials Science and Engineering, Shanghai Jiao Tong University

ANNOST 07 - SEPTEMBER 1 2017  
BIOMETAL  
Symposium on Biodegradable Metals for Biomedical Applications

## Stress corrosion of cold drawn and aged WE43 wires in different setups

P Maier<sup>1</sup>, AJ Griebel<sup>2</sup>, WD Mueller<sup>3</sup>, JE Schaffer<sup>2</sup>  
<sup>1</sup>University of Applied Sciences Stralsund, Stralsund, Germany. <sup>2</sup>Fort Wayne Metals Research Products Corp., Fort Wayne, IN, USA. <sup>3</sup>Charite Berlin, Universitätsmedizin, Germany

2019 Magnesium Technology

[Magnesium Technology 2019](#) pp 175-181 | [Cite as](#)

## Corrosion Bending Fatigue of RESOLOY<sup>®</sup> and WE43 Magnesium Alloy Wires

Authors [Authors and affiliations](#)

Petra Maier , Adam Griebel, Matthias Jahn, Maximilian Bechly, Roman Menze, Benjamin Bittner, Jeremy Schaffer

ELSEVIER

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Volume 113, 1 September 2020, Pages 627–645

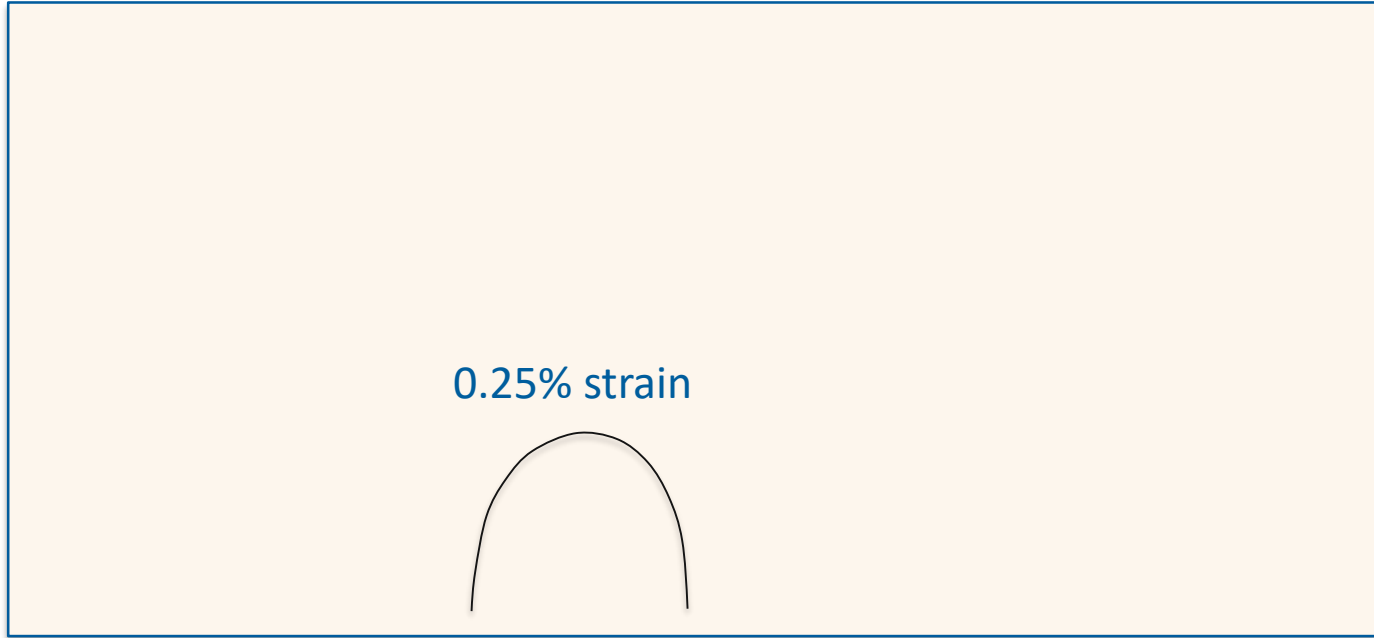
Full length article

## Effect of strain on degradation behaviors of WE43, Fe and Zn wires

Kai Chen <sup>a, b, 1</sup>, Yun Lu <sup>a, b, 1</sup>, Hongyan Tang <sup>a, b</sup>, Yuanming Gao <sup>a, b</sup>, Feng Zhao <sup>a, b</sup>, Xuenan Gu <sup>a, b</sup>, Yubo Fan <sup>a, b, c</sup>

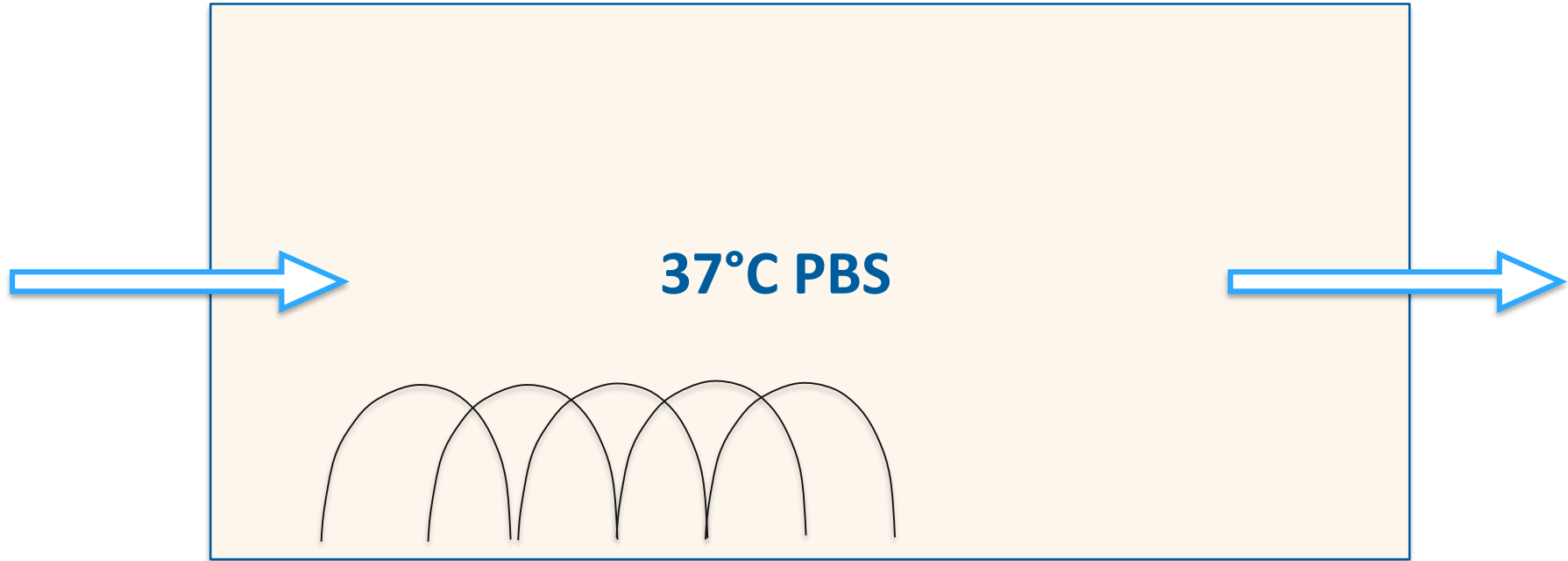


# Strain-Corrosion at FWM

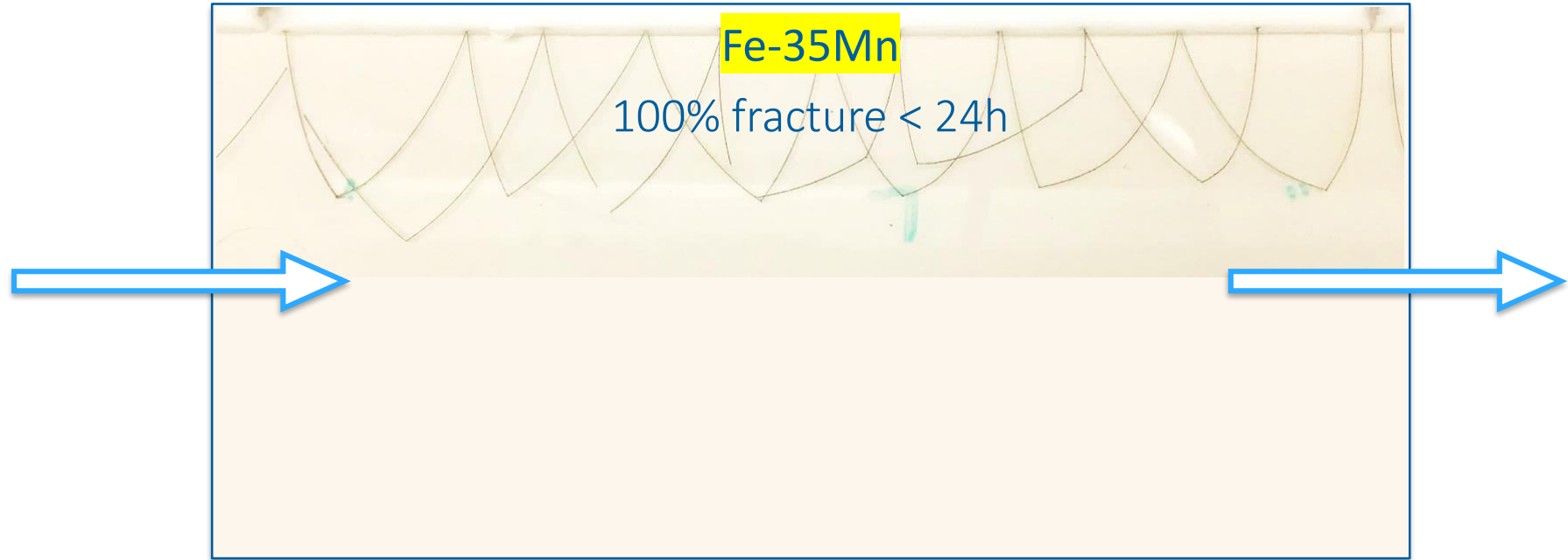




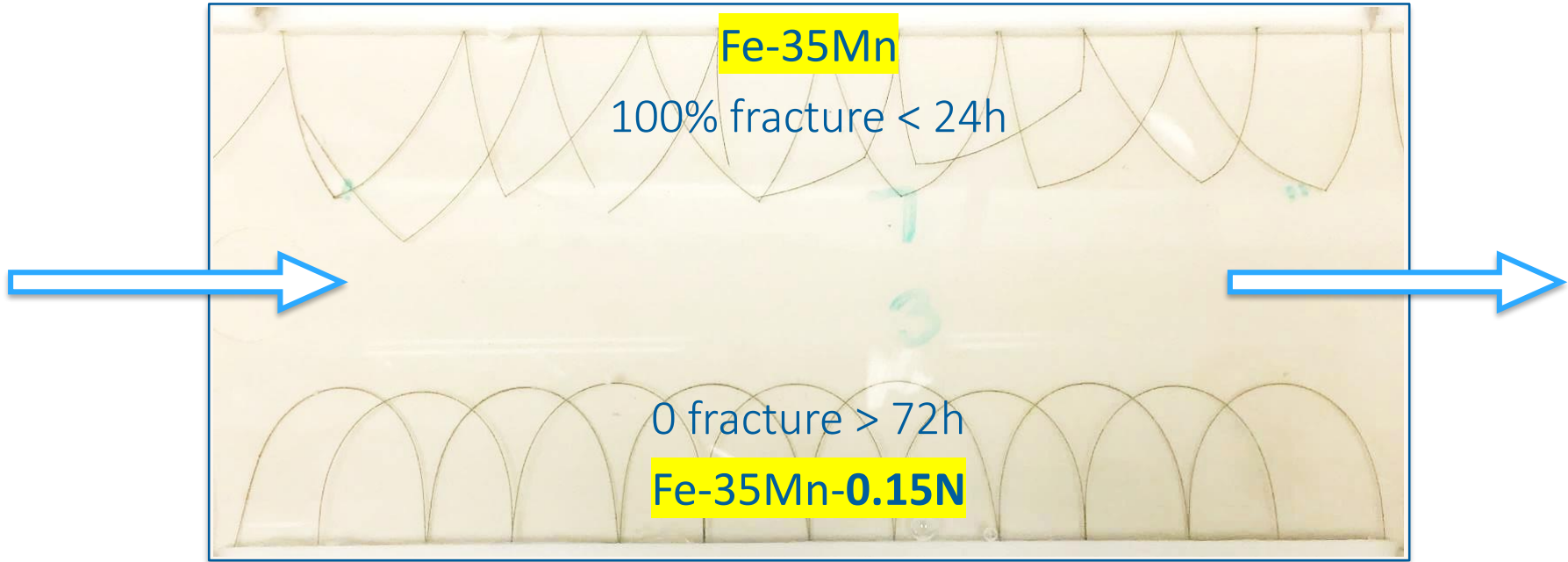
# Static strain-corrosion



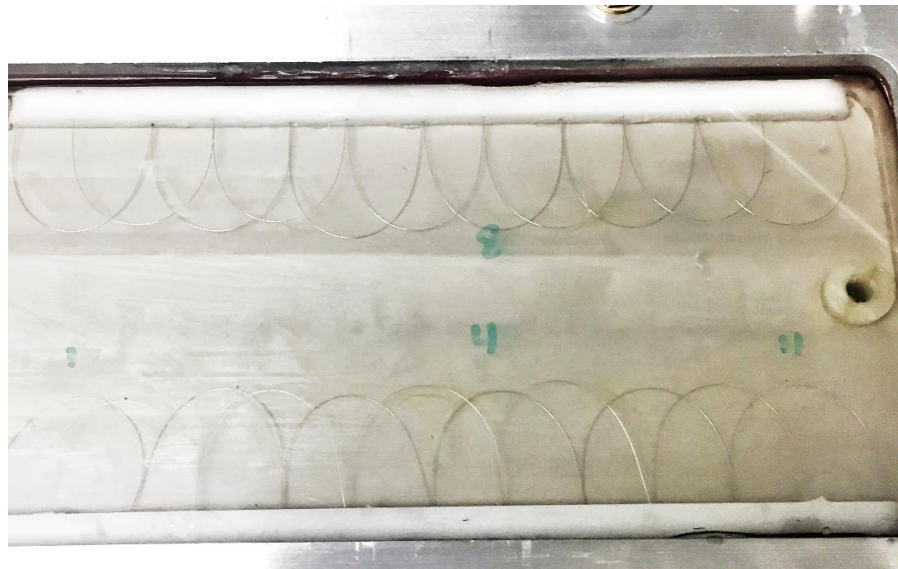
# Static strain-corrosion



# Static strain-corrosion



# Strain-controlled corrosion: Mg (WE43)



0 hrs



96 hrs

# Aim

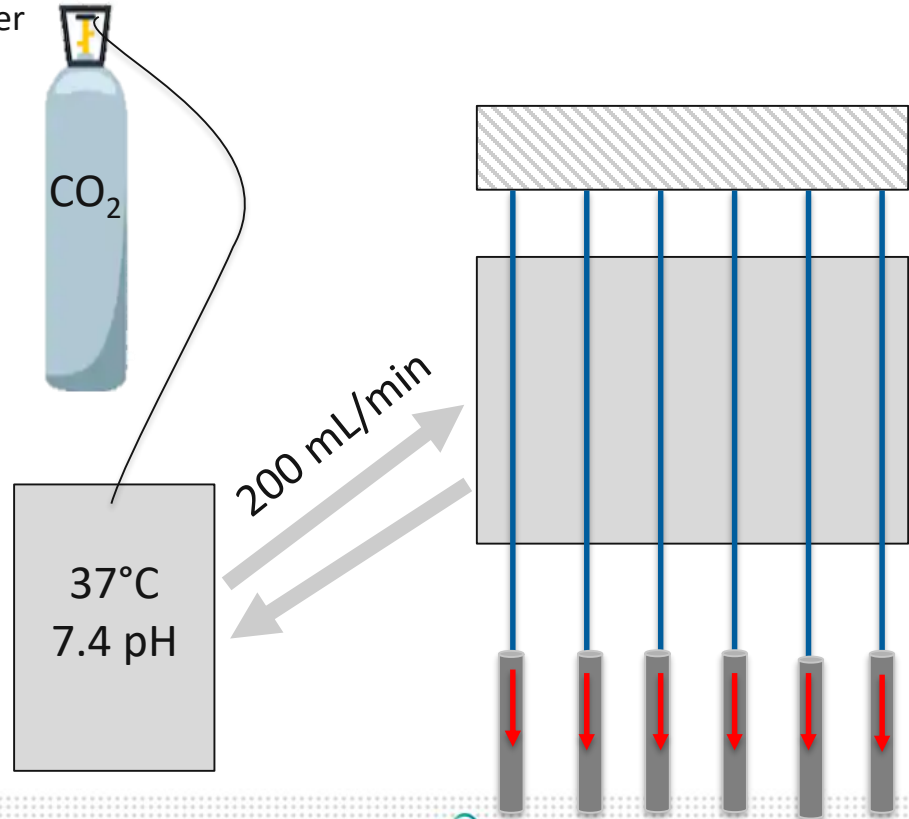
A corrosion testing method that can efficiently and repeatably assess corrosion and stress-corrosion behavior of fine Mg wires



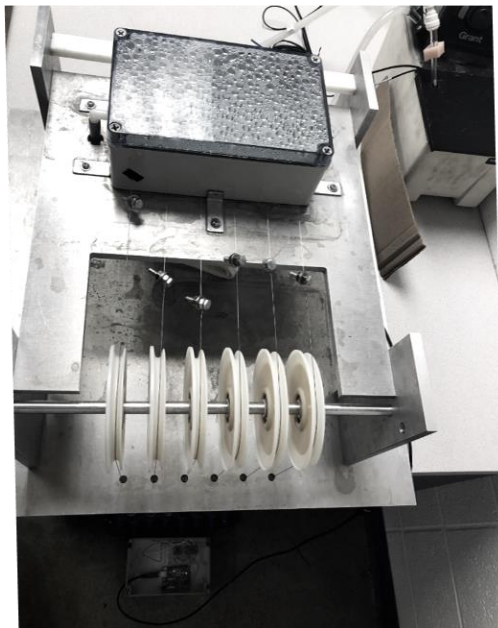


# Stress-Corrosion System Design

- 6 horizontal wires through 150 mm test chamber
- Stainless steel deadweights
- Electrical contact break detection system
- Media
  - 5L of Modified Hank's Solution
    - 1.6 g/L sodium bicarbonate
    - 0.265 g/L calcium chloride dihydrate
  - pH 7.4 +/- 0.1
    - Buffered with CO<sub>2</sub> bubbling
  - 37 +/- 1°C
  - 200 mL/min flow
- Data Outputs:
  - Time-to-failure
  - Post-corrosion cross-sectional analysis



# Stress-Corrosion System Design



# Test Plan

- Case 1: Compare alloys and process conditions at a given stress
- Case 2: Investigate influence of stress on corrosion rate at a given time
- Case 3: Generate stress-life curve for a given alloy and evaluate corrosion morphology



# Alloys Investigated

<b><u>Name</u></b>	<b><u>Mg</u></b>	<b><u>Li</u></b>	<b><u>Zn</u></b>	<b><u>Ca</u></b>	<b><u>Y</u></b>	<b><u>Nd</u></b>	<b><u>Zr</u></b>	<b><u>Mn</u></b>	<b><u>Fe</u></b>	<b><u>Cu</u></b>	<b><u>Ni</u></b>
<b>LZ21</b>	96.0	2.0	1.21	0.35	< 0.01	< 0.01	< 0.01	0.4	0.004	< .001	< .001
<b>WE43</b>	92.8	< 0.01	< 0.01	< 0.01	3.9	3.0	0.3	< .01	0.004	0.008	0.001
<b>L4</b>	96.4	3.5	< 0.01	0.01	< 0.01	< 0.01	< 0.01	0.03	0.004	0.008	<.001
<b>ZX10</b>	98.6	< 0.01	1.03	0.26	< 0.01	< 0.01	< 0.01	0.12	< .001	0.001	< .001




# Wire Production

- VIM, cast to  $\varnothing 50$  mm
- Extruded to  $\varnothing 12.7$  mm
- Wire drawing to  $\varnothing 0.24, 0.25$  mm



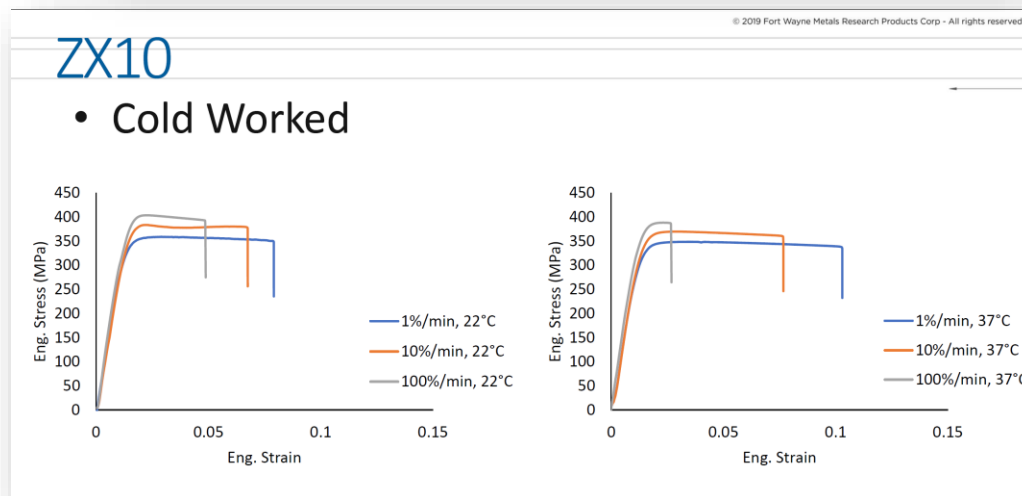


# Tensile Properties




11<sup>th</sup> BIOMETAL  
August 25 to 30, 2019  
Hotel Alcazar Golf  
Pinar del Rio, Spain

**Influence of Test Parameters on Tensile Properties of Magnesium Alloy Wire**  
Adam Griebel<sup>1</sup>, Jeremy Schaffer<sup>1</sup>  
<sup>1</sup> [Fort Wayne Metals](#), Fort Wayne, IN, USA



# Tensile Properties

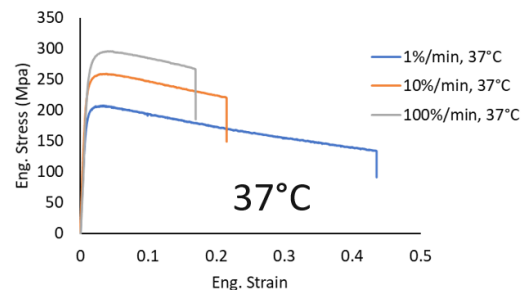
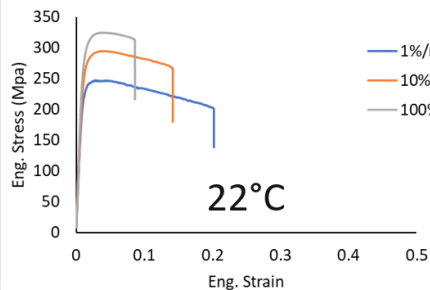


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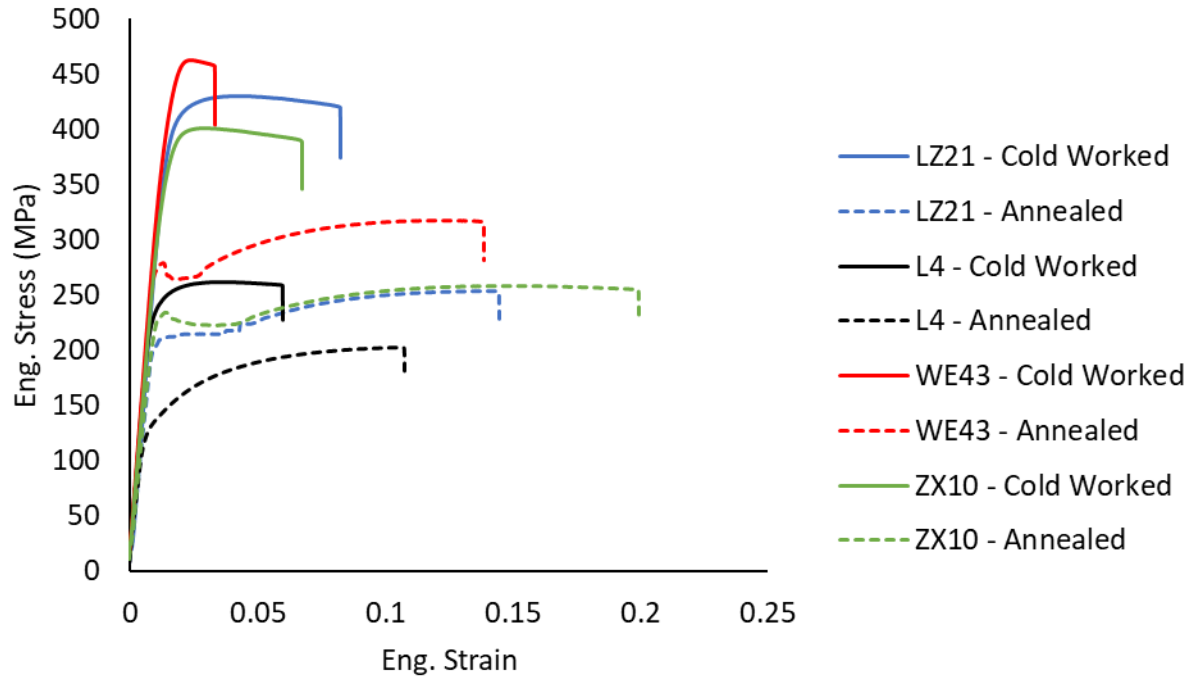
## Mg4Li

- Cold Worked



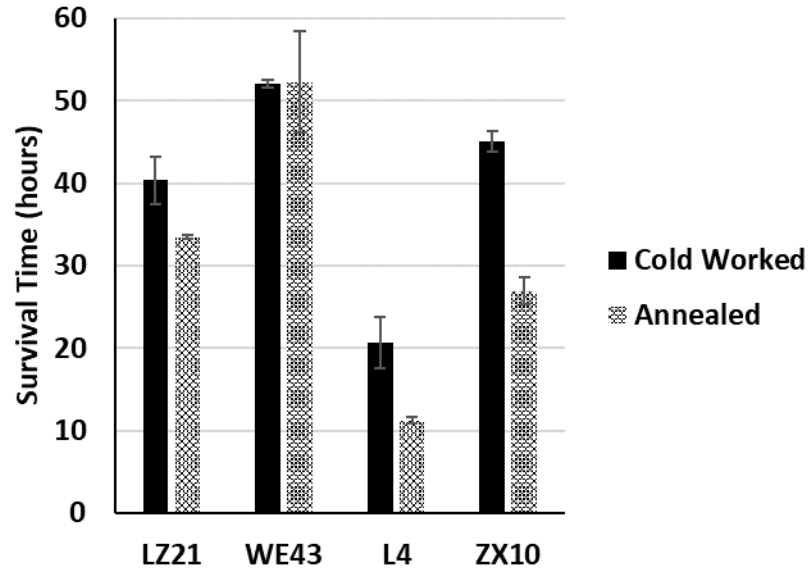
# Mg wire tensile

- 127 mm GL, 20%/min, 22°C



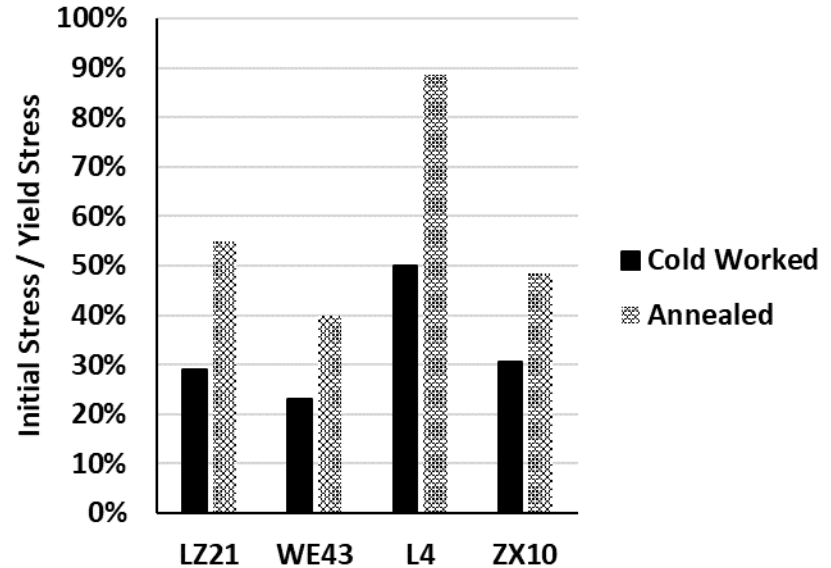
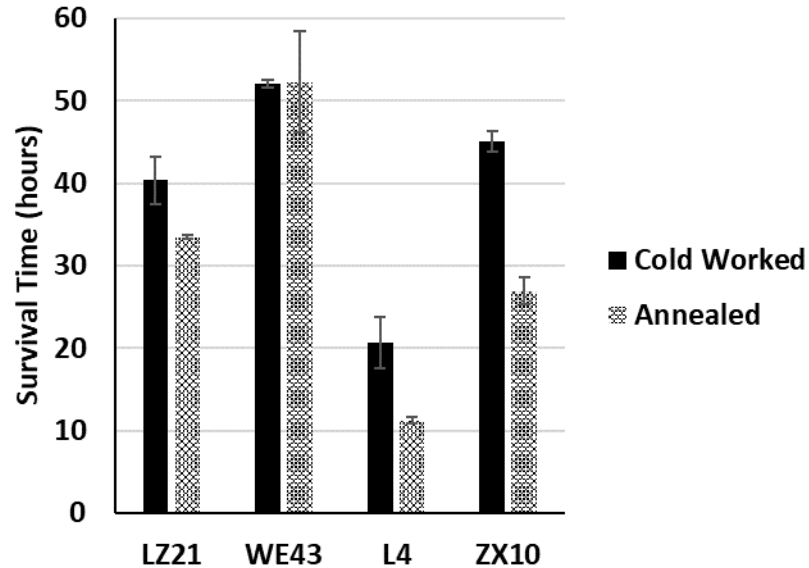
# Case 1: Comparing Alloys

- LZ21, WE43, L4, ZX10
  - 0.24 mm, 110 MPa initial stress, Both Cold Worked and Annealed conditions



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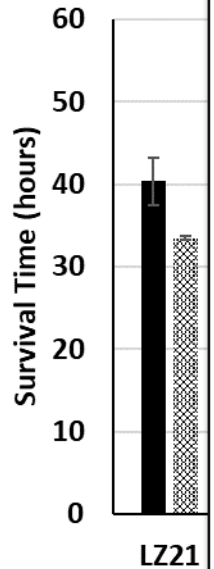




# Case 1: Comparing Alloys

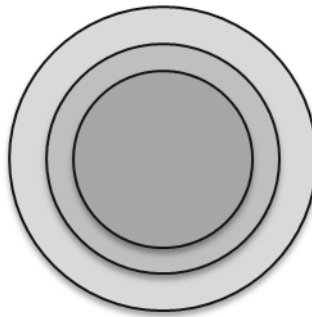
- LZ21, WE

– 0.24 mm



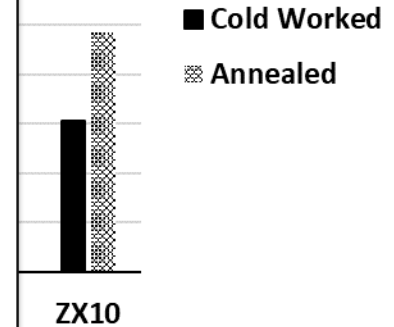
## Constant Force ≠ Constant Stress

$$\text{Stress} = \frac{\text{Force}}{\text{Area}}$$



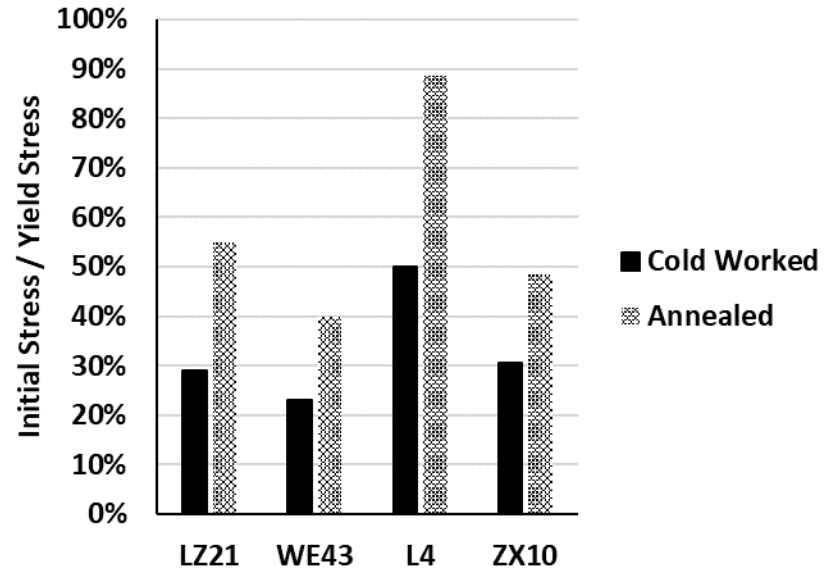
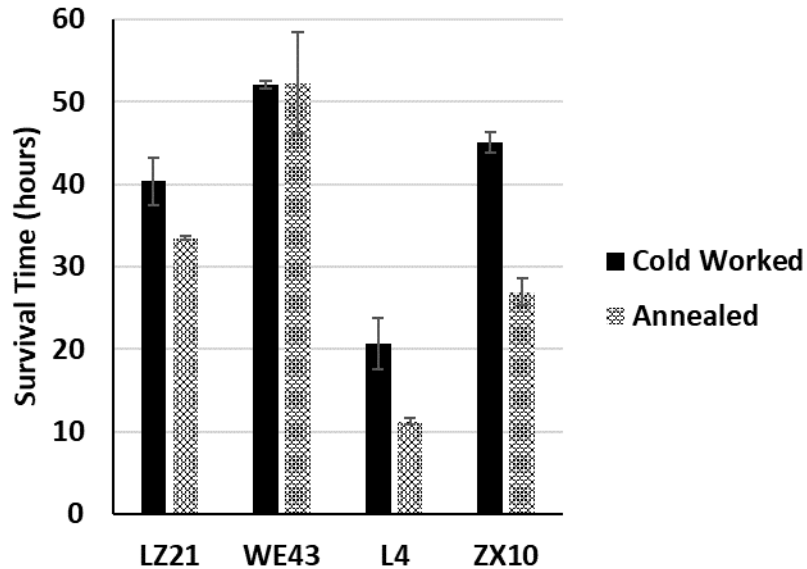
Wire corrodes → area decreases → stress increases

and conditions



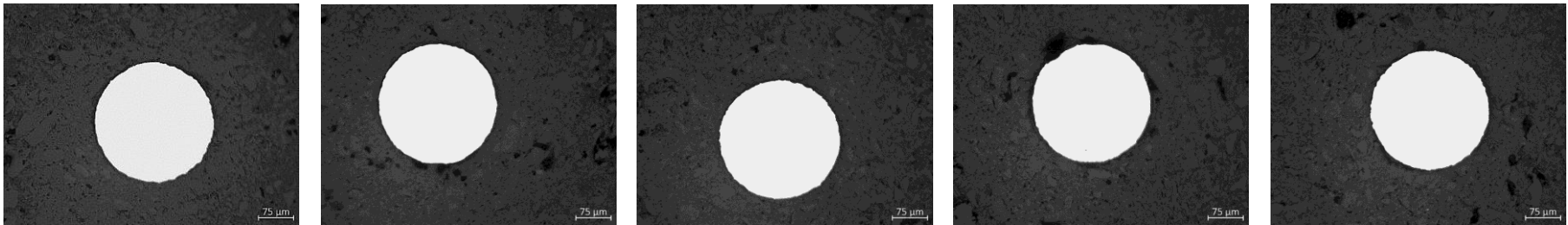
# Case 1: Comparing Alloys

- LZ21, WE43, L4, ZX10
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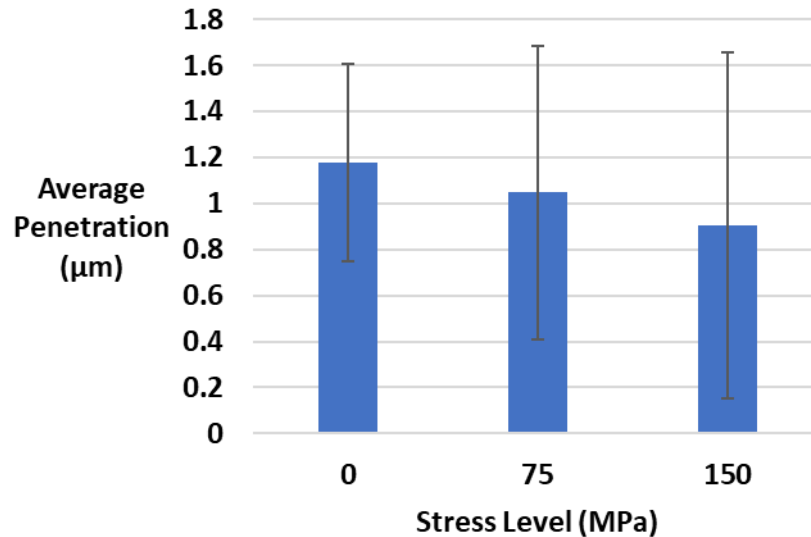
# Case 2: Influence of Stress

- 0.25 mm ZX10, cold worked, 16 hours
- Stress = 0, 75, 150 MPa
- Analysis:
  - Collect 5-6 cross-sections (mount/polish)
  - Measure remaining metal area and maximum penetration in ImageJ
    - Calculate Average Penetration and Pitting Factor.



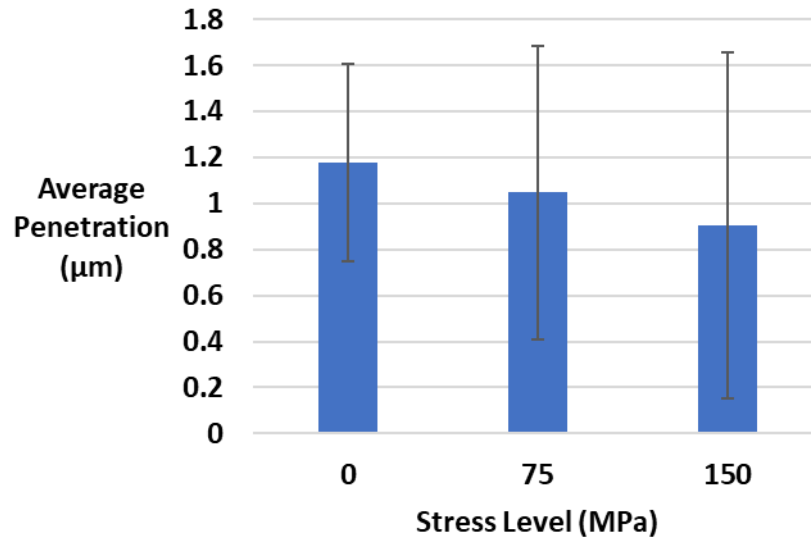
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# Case 2: Influence of Stress

- 0.25 mm ZX10, cold worked, 16 hours
- Stress = 0, 75, 150 MPa



Stress does not increase corrosion rate(?)

# Case 3: Stress-Life Curve

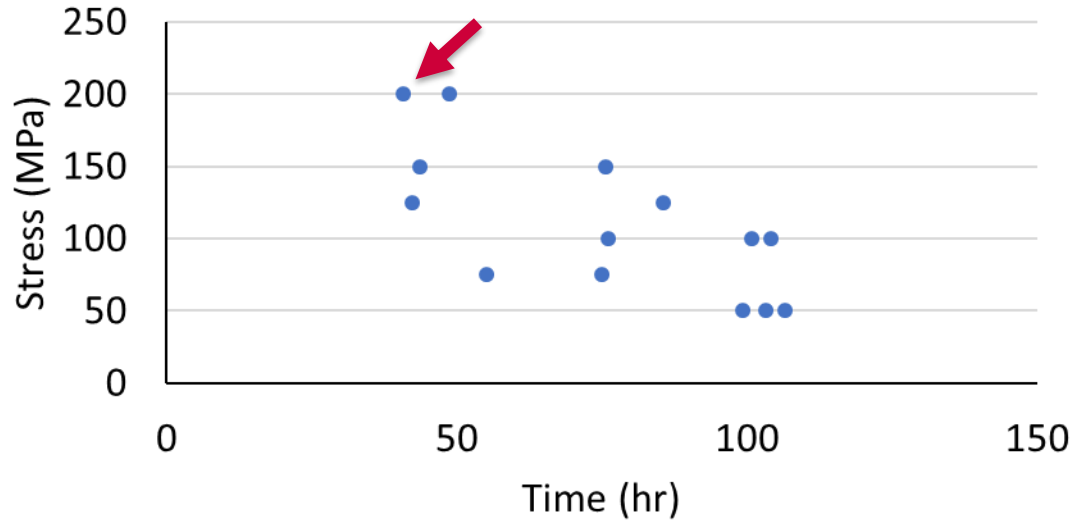
- 0.25 mm ZX10, cold worked
- Held at initial stresses of 50-200 MPa
- Outputs:
  - Survival time
  - Cross-sectional analysis





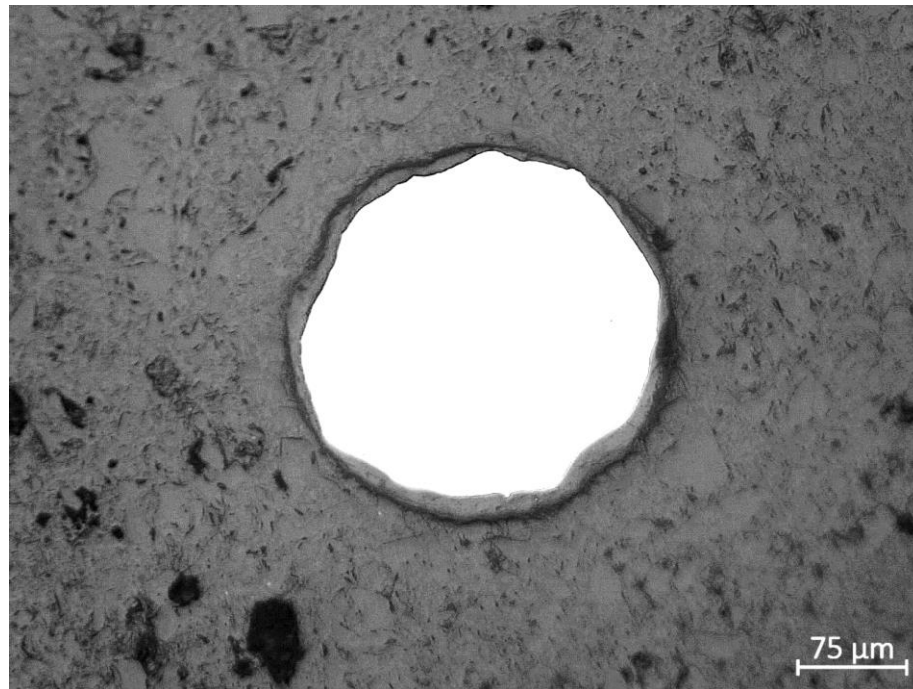
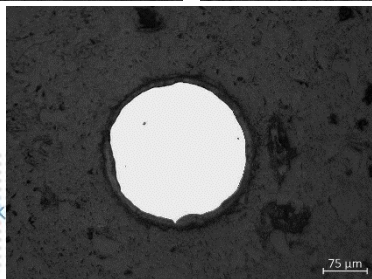
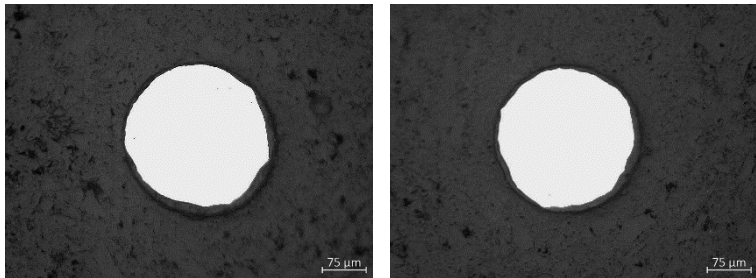
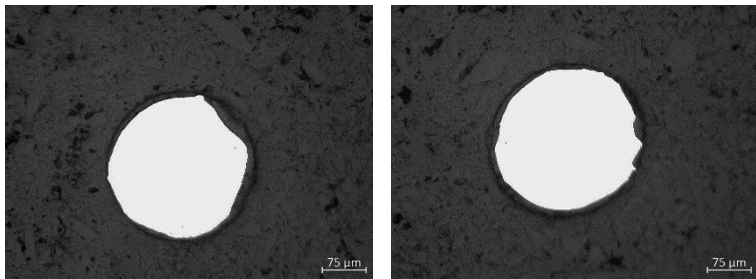
# Case 3: Stress-Life Curve

- 0.25 mm ZX10, cold worked



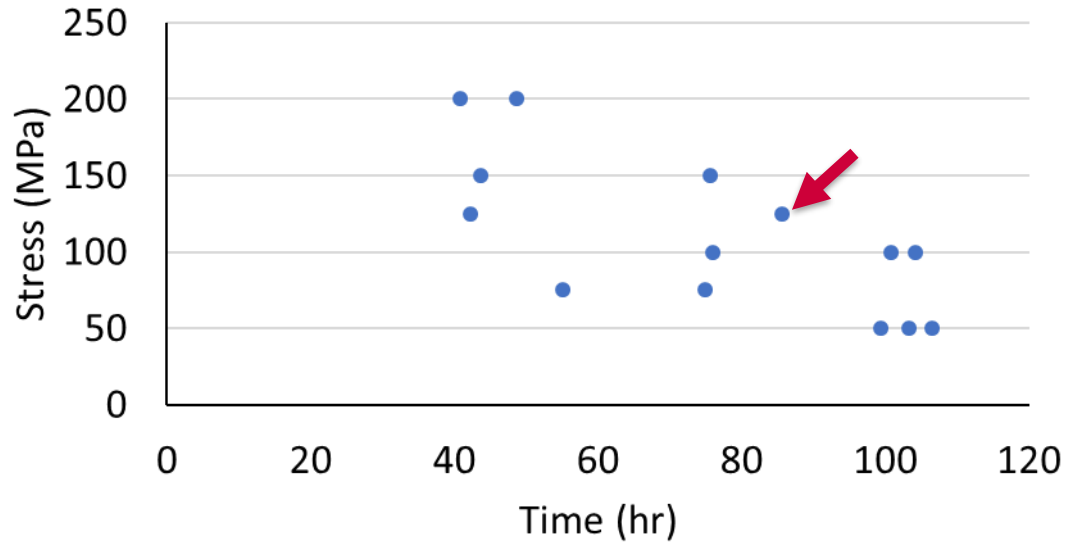
# Case 3: Stress-Life Curve

- 200 MPa, 40.8 hours



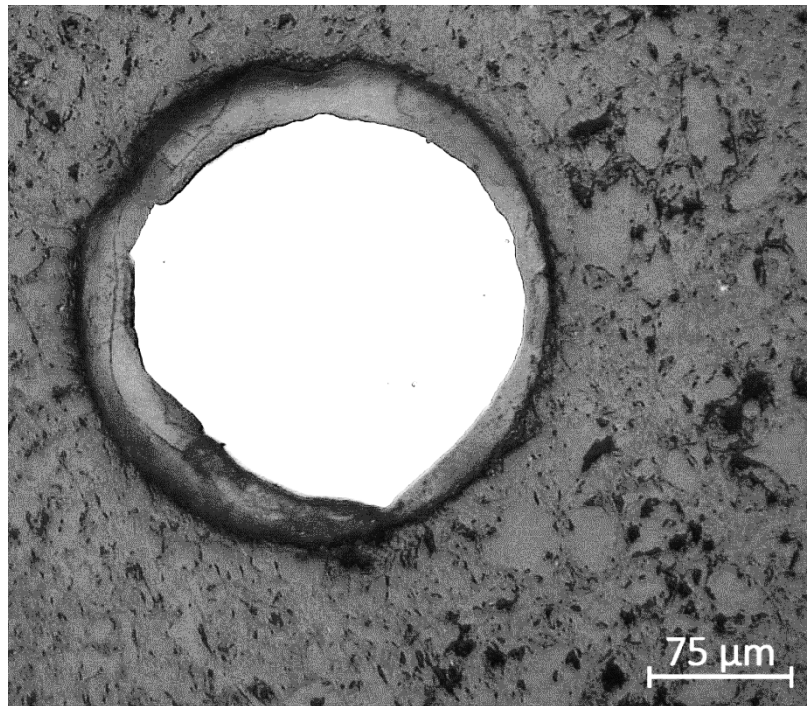
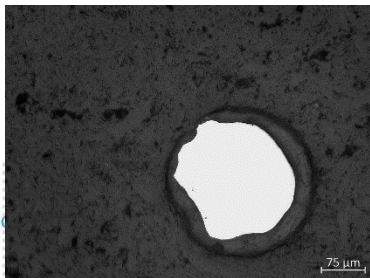
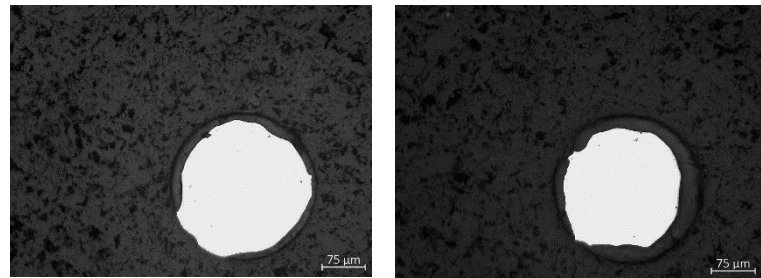
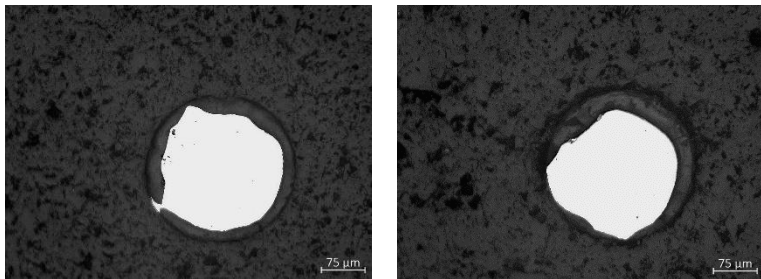
# Case 3: Stress-Life Curve

- 0.25 mm ZX10, cold worked



# Case 3: Stress-Life Curve

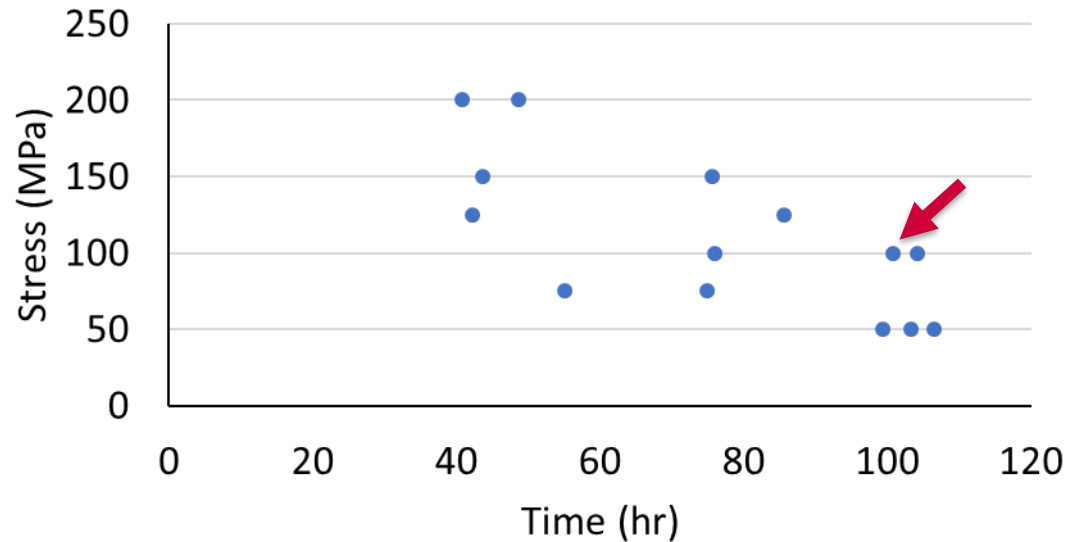
- 125 MPa, 85.6 hrs





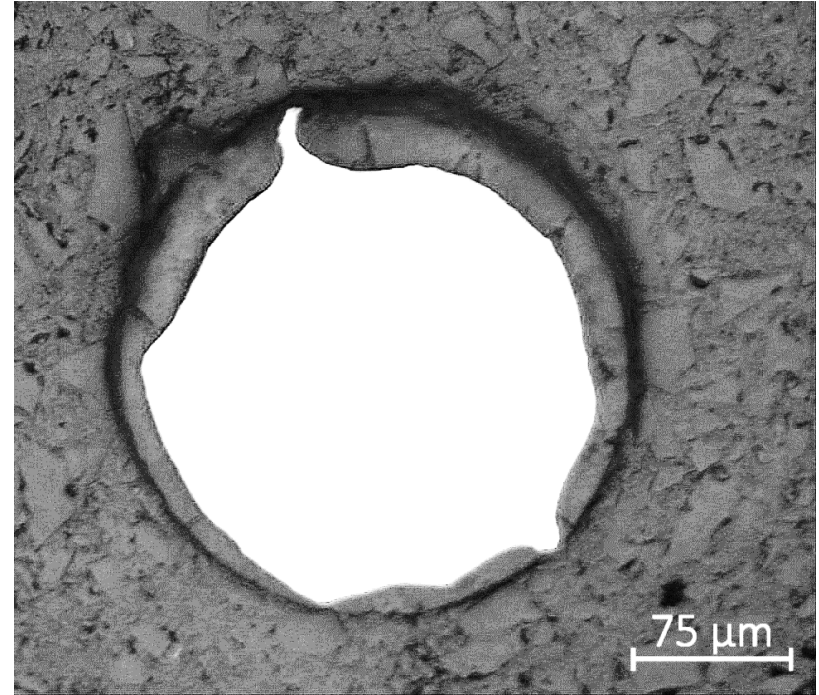
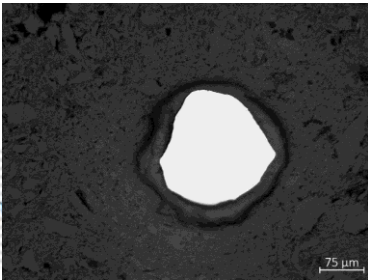
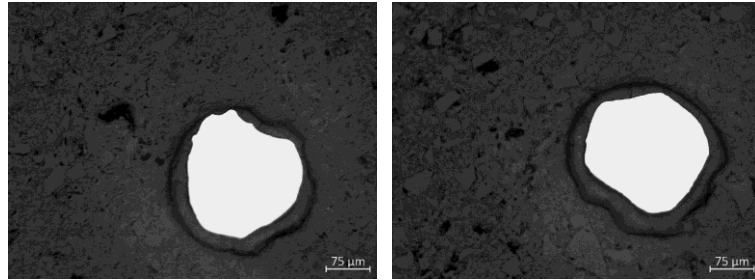
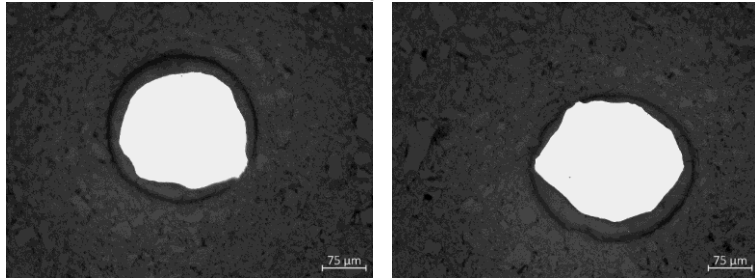
# Case 3: Stress-Life Curve

- 0.25 mm ZX10, cold worked



# Case 3: Stress-Life Curve

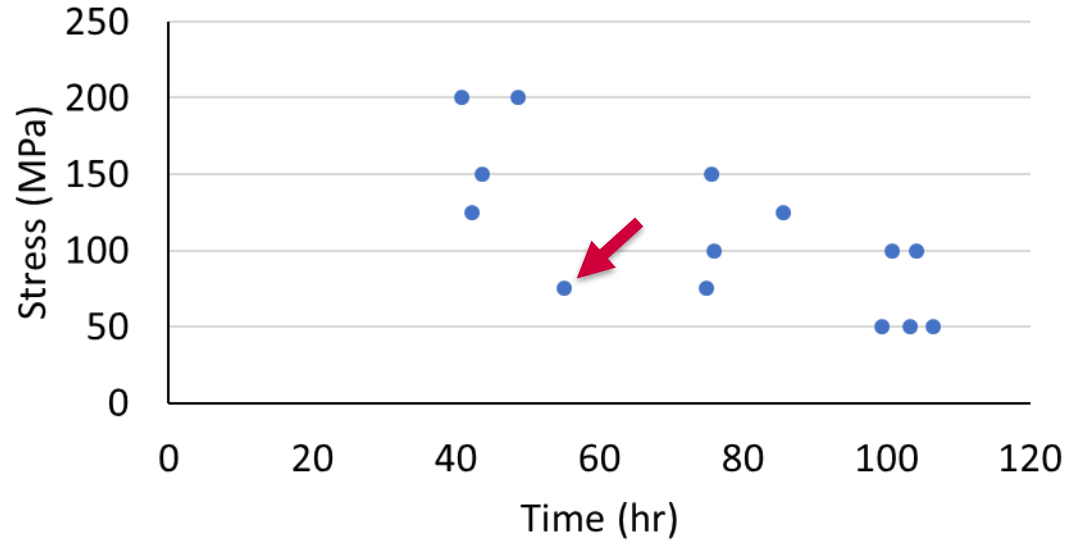
- 100 MPa, 100.8 hrs





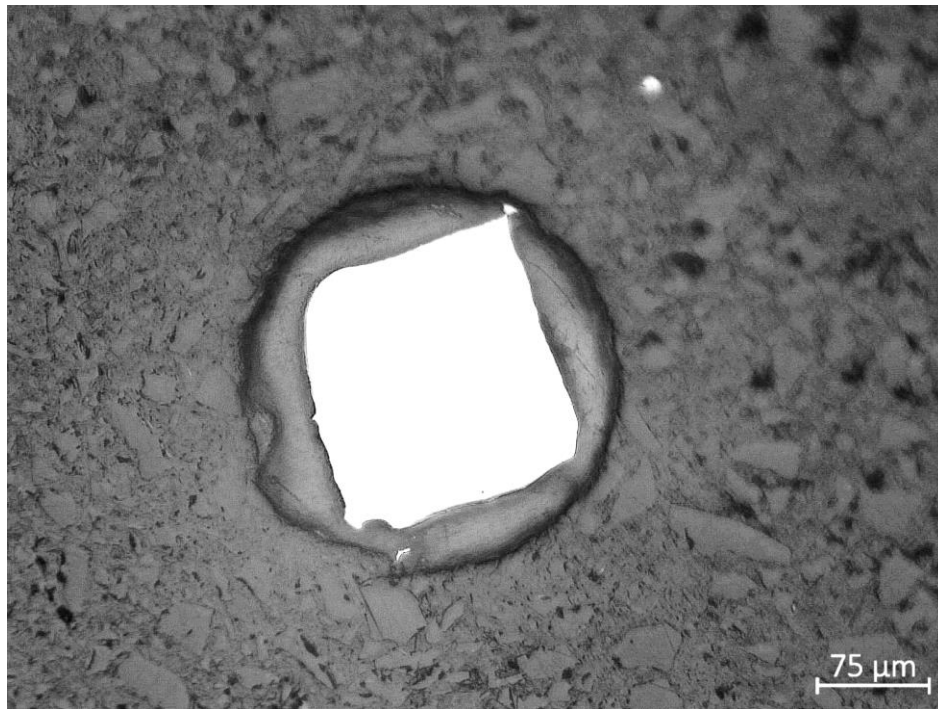
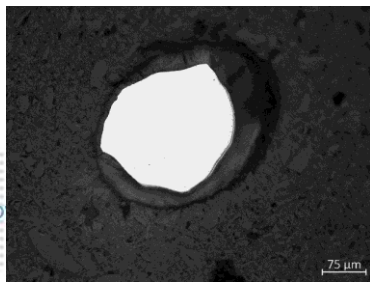
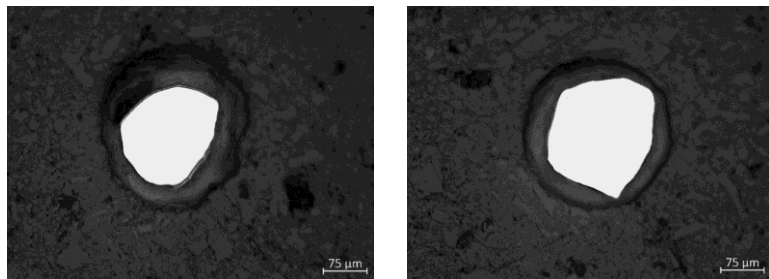
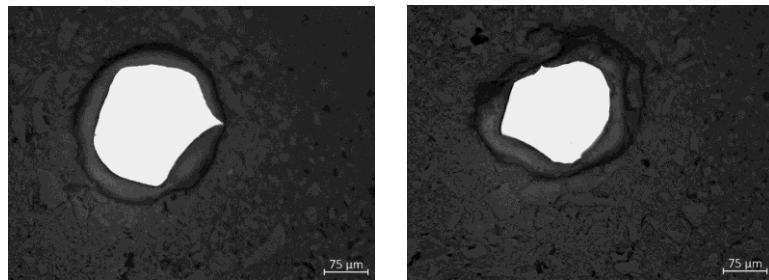
# Case 3: Stress-Life Curve

- 0.25 mm ZX10, cold worked

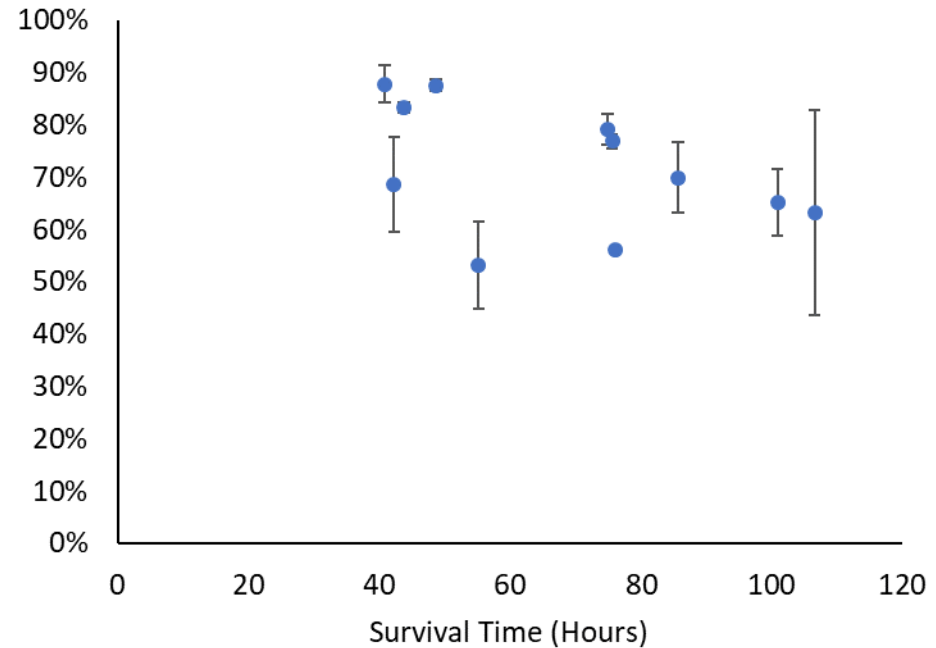
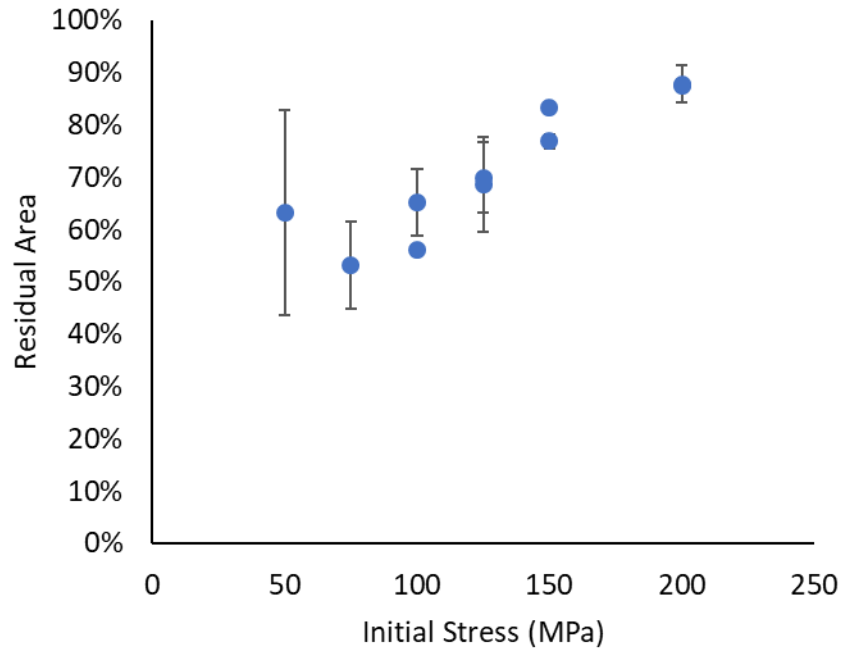


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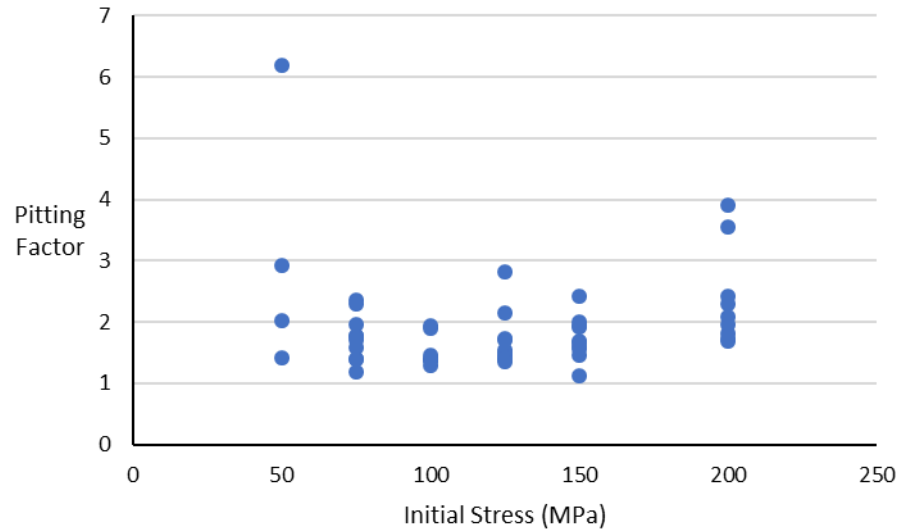
- 75 MPa, 55 hrs



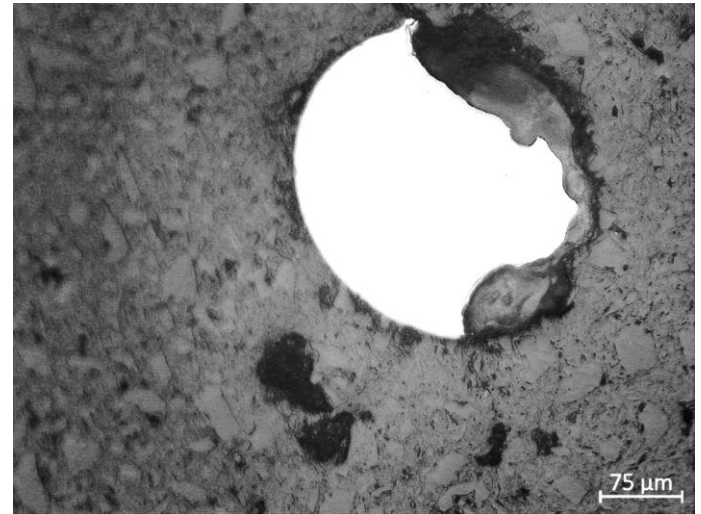
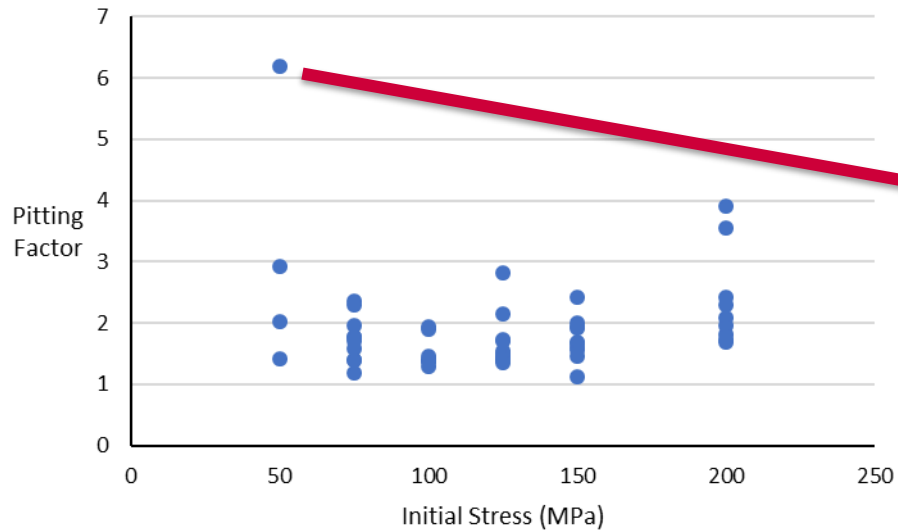
# Case 3: Residual Area



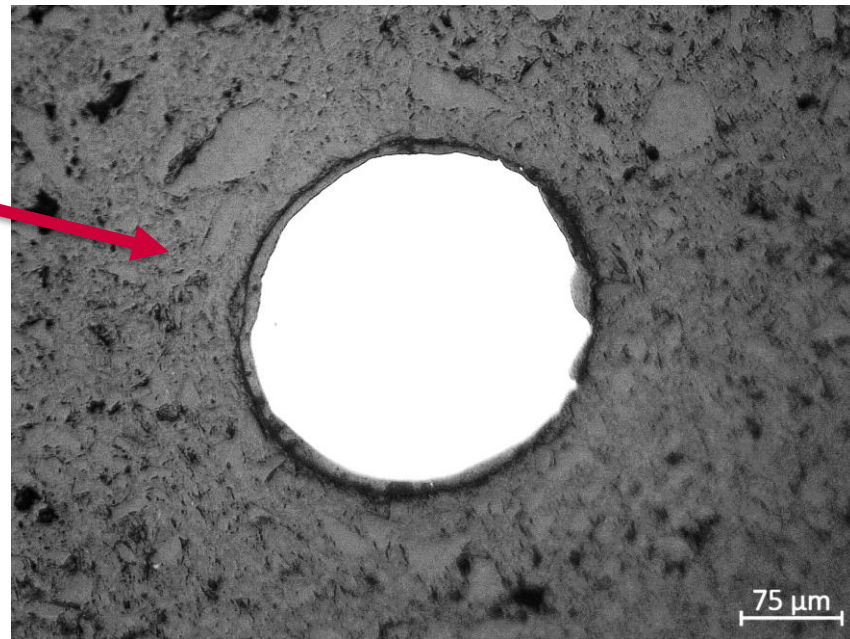
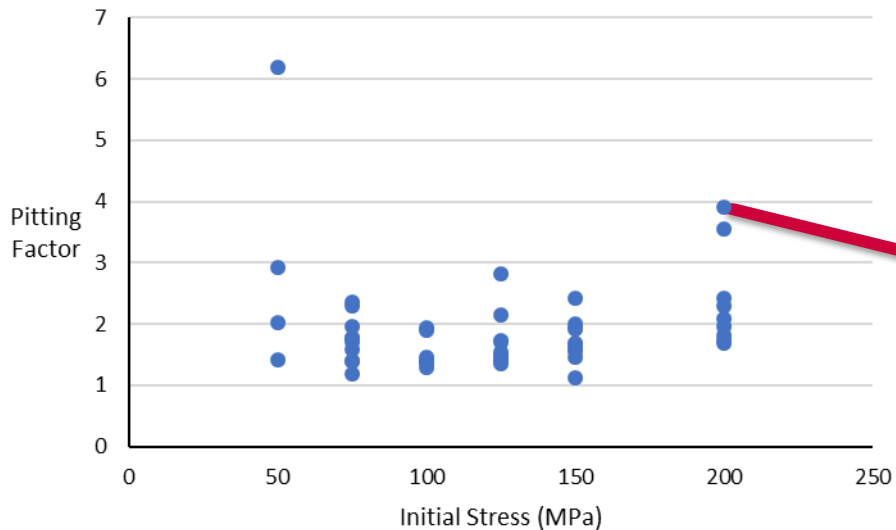
# Case 3: Pitting Factor



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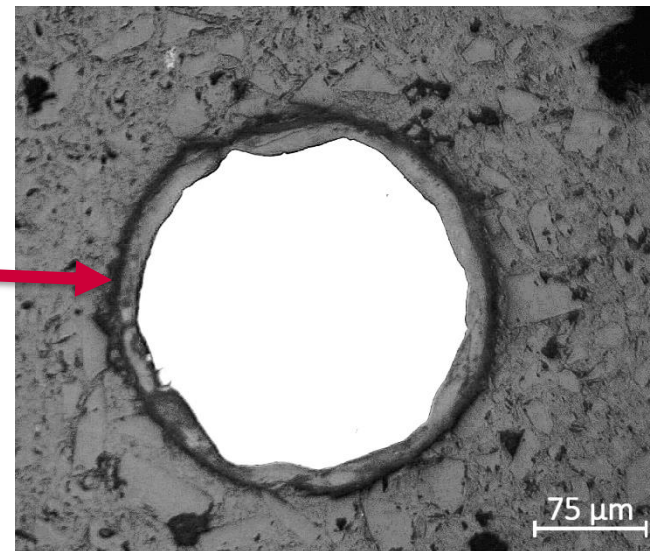
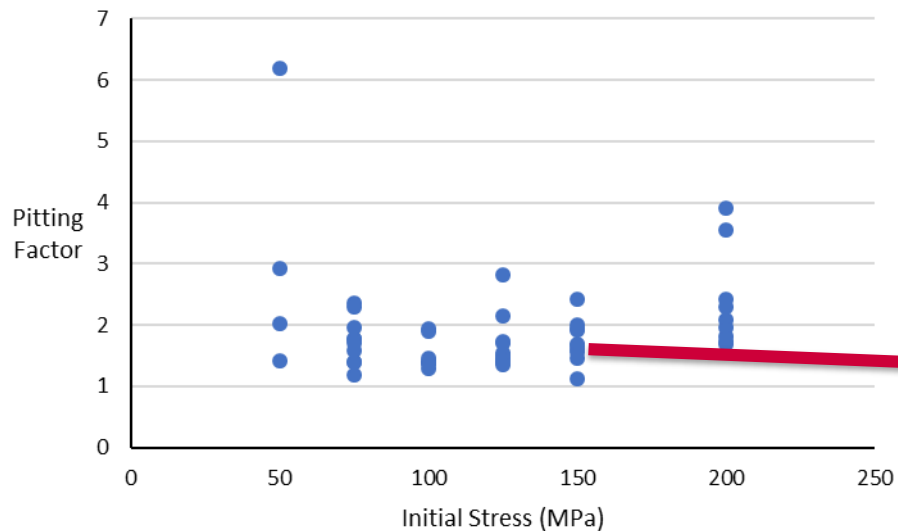


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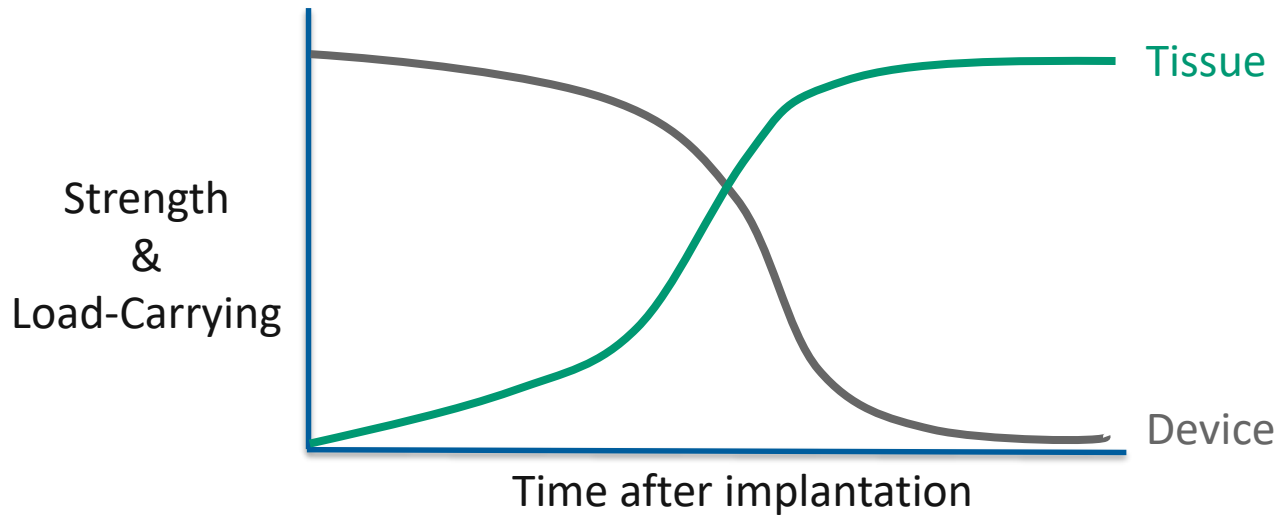




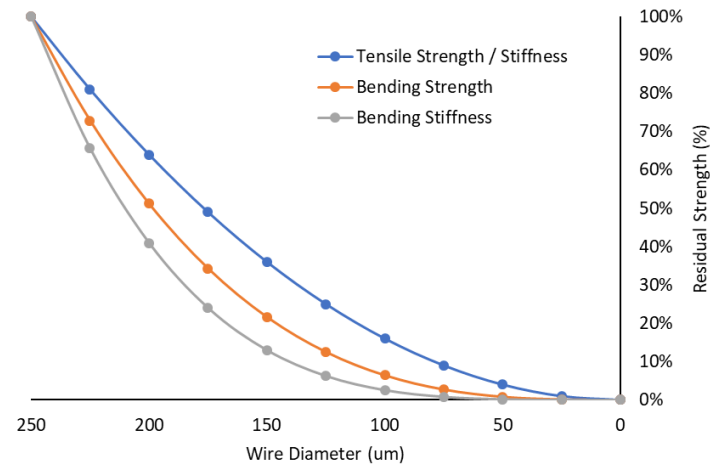
# How does this aid in the development of absorbable devices?



# Mechanical Transfer



# Actual loading depends on device



# Future work

- Case 1: Comparing Alloys
  - Confounding influence of strength
  - Hold constant time (pre-failure)
- Case 2: Does stress increase corrosion?
  - Longer duration (e.g. 36 hrs)
  - Additional alloys
- Case 3: Stress-Life curve
  - Additional alloys
  - Higher N
- Additional Studies
  - Microstructure vs corrosion (grain size, secondary phases)
  - Effect of impurities (Fe/Ni/Cu)
  - Surface/Coatings
  - Mechanical strength after set time



# Conclusions

- A simple stress-corrosion system was designed for testing of Mg alloy wires.
- The method
  - Effectively distinguishes Mg alloys and process conditions
  - Enables corrosion uniformity assessment
  - Will allow for efficient corrosion checks in a manufacturing environment



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ISO

ICS > 11 > 11.040 > 11.040.40

# ISO/TS 20721

## Implants for surgery – General guidelines and requirements for assessment of absorbable metallic implants

### GENERAL INFORMATION

Status : Under development Publication date : 2020-09

Edition : 1

Technical Committee : ISO/TC 150 Implants for surgery

ICS : 11.040.40 Implants for surgery, prosthetics and orthotics

### LIFE CYCLE

A standard is reviewed every 5 years

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# Thank you!

See you in 2021!

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